

## Formulation and Evaluation of an Oral Floating Tablet of Cephalexin

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### Abstract

The objective of this study was to formulate an oral floating tablet of cephalexin (CEF) using the hydrophilic polymer hydroxy propyl methyl cellulose (HPMC), gas generating agent sodium bicarbonate and citric acid. A  $3^2$  factorial design was applied systematically; the amount of citric acid (X1) and amount of HPMC K100M (X2) were selected as independent variables. The time required for 50% drug release ( $t_{50\%}$ ), percentage drug release at 12hr ( $Q_{12}$ ) and percentage drug release at 6 hr ( $Q_6$ ) were selected as dependent variables. The results of factorial design indicated that high level of HPMC K100M and citric acid favors preparation of floating sustained release tablet of cephalexin. The granules were prepared by wet granulation method and evaluated for their granules properties. Tablets were compressed by KBr press and evaluated with different parameters like diameter, thickness, average weight, hardness, friability, drug content, in vitro buoyancy study, swelling characteristics, scanning electron microscopy, kinetic release data. Hardness was found to be in the range of  $13 \pm 0.23$  to  $13 \pm 0.40$  kg/cm<sup>2</sup>, the percent friability was in the range of  $0.0010 \pm 0.02$  to  $0.0027 \pm 0.01$ , and tablets showed  $99.63 \pm 0.12$  to  $115.73 \pm 0.13$  of the labeled amount of cephalexin indicating uniformity content. The tablets containing CEF released 72.28 to 99.461 % of drug at the end of 12 hr by in vitro release study. The drug release followed the Korsmeyer and Peppas model controlled mechanism of cephalexin tablet.

**Keywords** Cephalexin, Hydroxy propyl methyl cellulose, gastroretentive, floating drug delivery, sustained release

### INTRODUCTION

Oral delivery of drugs is by far the most preferable route of drug delivery due to the ease of administration, patient compliance and flexibility in formulation etc. From immediate release to site specific delivery, oral dosage forms have really progressed. Gastroretentive dosage forms significantly extend the period of time, over which drug may be released and thus prolong dosing intervals and increase patient compliance. Such retention systems are important for those drug that are degraded in the intestine like antacids or certain antibiotics, enzymes that act locally in the stomach. These systems can be retained in the stomach and assist in improving the oral sustained delivery of drugs that have an absorption window in a particular region of the gastrointestinal tract, thus ensuring optimal bioavailability.<sup>1,2</sup> Various gastroretentive techniques were used, including floating, swelling, high density, and bioadhesive system, have

been explored to increase the gastroretention of dosage forms<sup>3,4</sup>. Floating systems having low density systems that have sufficient buoyancy to float over the gastric contents and remain in the stomach without affecting the gastric emptying rate for a prolonged period. While the system floats over the gastric contents, the drug is released slowly at the desired rate, which results in increased gastric retentive time and reduces fluctuation in plasma drug concentration.<sup>5,6</sup>

Formulation of floating tablet containing cephalexin as a drug candidate, which would remain in stomach or upper part of GIT for prolonged period of time, therefore the maximum drug release is maintained at desired site.<sup>7</sup> Cephalexin having good absorption in GIT, low pKa, which remain unionized in stomach for better absorption. Cephalexin is a semisynthetic cephalosporin  $\beta$  lactam antibiotic intended for oral administration used to treat urinary tract infections, respiratory tract infections, skin and soft tissue infections. Pharmacokinetic parameters of cephalexin such as absorption from the gastrointestinal tract, protein binding 14%, and metabolism 90% excreted

unchanged in the urine, half-life is 1 hour.<sup>8</sup> It degraded in alkaline pH, so as to prevent degradation, gastro retentive dosage forms can help in preventing degradation, which degrades in small intestine. Low viscosity hydrophilic polymers HPMC K100 were found to be more beneficial to improving floating properties. Hydrophilic polymer slowly forms thick gel, which retains integrity of the formulation and promotes drug release through thick gel which controls the burst release.<sup>9</sup> To investigate the effect of amount of citric acid and hydroxypropylmethyl cellulose K100M on the formulation to monitor the sustained release effect respectively.<sup>10</sup> For the present study cephalexin was selected as drug candidate, and HPMC K100 as polymer, both the drug and polymer fulfills the above characteristics, which indicate its suitability for fabrication into the floating drug delivery system.

#### MATERIALS AND METHODS

Cephalexin was received as a gift sample from Orchid Chemicals and Pharmaceutical (Chennai, India), Aurobindo Pharma, Hyderabad and Okasa Pharma, Satara. Hydroxy propyl methylcellulose K- 100M (HPMC- K100M) was obtained from Colorcon Asia Pvt Ltd (Goa, India) and Microcrystalline cellulose was received as a gift sample from Maple Biotech Pvt Ltd (Pune, India). Sodium bicarbonate, citric acid, magnesium stearate, talc were purchased from Poona Chemicals Laboratories (Pune, India). All other chemicals were of analytical grades as required.

#### Experimental:

##### Characterization of Cephalexin:

**Description:** The sample of cephalexin was analyzed for its nature, color and taste.

**Melting Point:** The melting point was taken by open capillary method.

**Standard Curve of Cephalexin:** Cephalexin has been quantitatively analyzed by various techniques. In present studies, Cephalexin was estimated by UV Spectrophotometry method.

**Infrared spectra analysis:** Infrared spectrum of Cephalexin was determined on Fourier Transform Infrared Spectrophotometer (FTIR-4100s) using KBr dispersion method. The base line correction was done using dried potassium bromide. Then the spectrum of dried mixture of drug and potassium bromide was run.

**Differential scanning calorimetry:** The Differential Scanning Calorimetric analysis was carried out using SDT 2960 TA Instrument, USA, Differential Scanning Calorimeter. Samples were placed in a platinum crucible and the DSC thermograms were recorded at a heating rate of 10°C/min in the range 20 °C to 350 °C, at a nitrogen flow of 20 ml/min.

#### Preparation of Floating Tablet of Cephalexin :

Each floating tablets containing 500mg cephalexin were prepared by a conventional wet granulation method, employing sodium bicarbonate, citric acid as gas generating agent and water-soluble polymer (HPMC K100M) as hydrophilic matrix in each formulation. (**Table No.1**) The concentration of gas generating agent (sodium bicarbonate) was developed as optimal concentration under experimental formulae and condition of preparation. All the ingredients were mixed thoroughly except magnesium stearate and talc. Granules were prepared manually with a solution of the of Polyvinyl pyrrolidone (PVP K30) in sufficient isopropyl alcohol as binder. The wet mass was passed through a 16 mesh sieve no. and the wet granules produced were dried in hot air oven for 30 min at 50°C. The dried granules mixed with magnesium stearate as lubricant, talc as glidant and compressed into tablet on a KBr press machine with 13mm punches. Prior to compression, granules were evaluated for their flow and compressibility characteristics.<sup>11-14</sup>

#### Full Factorial Design:

A 3<sup>2</sup> randomized full factorial design was used, in this design 2 factors were evaluated, each at 3 levels and experimental trials were performed at all 9 possible combinations. The amount of citric acid (X<sub>1</sub>) and amount of HPMC (X<sub>2</sub>) were selected as independent variables. The time required for 50% drug dissolution (t<sub>50%</sub>), percentage drug release at 12 hours (Q<sub>12</sub>) and percentage release at 6 hours (Q<sub>6</sub>) were selected as dependent variables.<sup>15-17</sup>

#### Evaluations of Granules Properties:

The flow properties of granules were characterized in terms of angle of repose, Carr index and Hausner's ratio. The bulk density and tapped density were determined and from this data Carr's index and Hausner's ratio were calculated.

### Evaluation of Tablet Properties:

The prepared cephalixin floating tablets were evaluated for thickness, diameter, hardness, friability, uniformity of weight and drug content. The thickness and diameter of tablets were measured by vernier caliper. Hardness of tablets was tested using Monsanto hardness tester. Friability of tablets was determined by using Friability test apparatus. The drug content in each formulation was determined by taking 20 tablets from each batch were weighed and powdered. The powder equivalent to 10 mg was taken and dissolved in 10 ml 0.1 N HCl. This stock solution was shaken for 20 min. on a sonicator. This resulting solution is further diluted with 0.1 N HCl to achieve concentration up to 10 g/ml and the absorbance measured at the 257 nm.<sup>18-20</sup>

### In-Vitro Buoyancy Study:

The in-vitro buoyancy study was characterized by floating lag time and total floating time. The test was performed using a USP type II paddle apparatus (Electrolab) using 900 ml of 0.1 N HCl at paddle rotation of 50 rpm at  $37 \pm 0.5^\circ\text{C}$ . The time required for the tablet to rise to the surface of the dissolution medium and the duration of time the tablet constantly floated on the dissolution medium were noted as floating lag time and total floating time respectively.<sup>21,22</sup>

### Swelling Characteristics (Water Uptake Study):

The swelling properties of HPMC matrices containing drug were determined by placing the tablet matrices in the dissolution test apparatus, in 900 ml of 0.1 N HCl at  $37 \pm 0.5^\circ\text{C}$ . The tablets were removed periodically from dissolution medium. After draining free from water by blotting paper, these were measured for weight gain. Swelling characteristics were expressed in terms of percentage water uptake (WU %) show relationship between swelling index and time.<sup>23-26</sup>

$$\text{WU \%} = \frac{\text{Weight of swollen tablet} - \text{Initial weight of the tablet}}{\text{Initial weight of the tablet}} \times 100$$

### In Vitro Drug Release Study:

The release rate of cephalixin floating tablets were determined by using Dissolution testing apparatus USP type II (Paddle type)( Electro lab).<sup>27-29</sup> The dissolution testing was performed using 900ml of 0.1N HCl at  $37 \pm 0.5^\circ\text{C}$  temperature and speed 50 rpm. A sample (5ml) of the solution was withdrawn from the dissolution testing

apparatus hourly for 12 hours and the samples were replaced with fresh dissolution medium. The samples were filtered through a  $0.45\mu$  membrane filter and diluted to a suitable concentration with 0.1N HCl. Absorbance of these solutions was measured at 257 nm wavelength using JASCO UV530 spectrophotometer. Analysis of data was done by using 'PCP Disso V-3' software, India.

### Scanning Electron Microscopy:

The SEM images of the tablet has been used to examine surface topography, texture and morphology of fractured surface. SEM analysis was conducted using JOEL JSM-T330A scanning microscope for optimized formulation.

### RESULTS AND DISCUSSION

The sample of cephalixin was off white or almost, white, crystalline powder, odour characteristic. The reported melting point values for cephalixin are in the range of  $326.8^\circ\text{C}$ . The observed melting point ranged between  $321 - 324^\circ\text{C}$ . The absorption maximum of the standard solution was scanned between 200-400 nm regions on JASCO UV 530 spectrophotometer. The absorption maximum was found to be 257 nm.

Infrared absorption spectrum of Cephalixin: IR spectrum shows all prominent peaks of Cephalixin. IR spectrum indicated that characteristics peaks belonging to measure functional groups such as principle peaks at wave numbers 3335.12, 1686.44, 3054.69, 2525.12, 1196.61 and  $1282.43\text{ cm}^{-1}$ , The major IR peaks observed in Cephalixin were 3335.12 (3300-3500) (N-H), 1686.44 (1680 - 1760 (C=O), 3054.69 (3300 - 2500 (O-H), 2525.12 (2590 – 2550 (S-H), 1196.61 1220 -1020 (C-N) and  $1282.43(1000-1300)(\text{C-O})$  ( Fig. 1).

Infrared absorption spectrum of HPMC K 100: The spectrum shows all prominent peaks of HPMC K100M. IR spectrum indicated characteristics peaks belonging to measure functional groups such as principal peaks at wave numbers 2922.59, 3420.14, 1058.73,  $1640.16\text{ cm}^{-1}$  The major IR peaks observed in HPMC K100M were 2922.59 (2850 – 3000) (C-H), 3420.14 (3300 – 3500) (N-H), 1058.73 (1000 – 1300) (C-O)  $\text{cm}^{-1}$  ( Fig. 2).

Infrared absorption spectrum of Physical mixture: The IR spectra of physical mixture of polymers (HPMC K100M) and cephalixin was studied and confirmed that there is no interaction with each other. The spectra show all the prominent peaks of drug as well as polymer. IR spectrum indicated characteristics peaks belonging to

measure functional groups such as principal peaks at wave numbers 2884.02, 1757.8, 1594.84, 1353.78, 1070.3cm<sup>-1</sup>. The major IR peaks observed in matrices were 2884.02 (2850–3000) (C-H), 1757.8 (1680–1760) (C=O), 1594.84 (1550–1650) (N-H), 1353.78 (1350–1550) (N=O), 1070.3 (1000–1300) (C-O). Hence it can be concluded that there were no any significant changes and behavior in the physical mixture of cephalixin and polymer (HPMC K100M) (**Fig. 3**).

Differential Scanning Calorimetry: DSC thermogram of Cephalixin show endothermic peak at 327.5°C. Where as HPMC K100M show melting endothermic peak at 34.40°C. Physical mixtures show endothermic and exothermic peak at 105°C and 190°C respectively. While optimized batch also show the endothermic peak at 70.7°C and 180.2°C (**Fig. 4**).

A 3<sup>2</sup> factorial design was constructed to study the effect of the amount of citric acid (X<sub>1</sub>) and HPMC K100M (X<sub>2</sub>) on the drug release from floating cephalixin tablet respectively. The dependent variables chosen were times required for 50% drug release (t<sub>50%</sub>), percentage drug release at 12 hours (Q<sub>12</sub>) and percentage drug release at 6 hours (Q<sub>6</sub>) given in (**Table 2**). A statistical model incorporating interactive and polynomial term was used to evaluate the responses.

$$Y = b_0 + b_1X_1 + b_2X_2 + b_{12}X_1X_2 + b_{11}X_1^2 + b_{22}X_2^2$$

Where, Y is dependent variable, b<sub>0</sub> is the arithmetic mean response of the 9 runs, and b<sub>i</sub> (b<sub>1</sub>, b<sub>2</sub>, b<sub>12</sub>, b<sub>11</sub> and b<sub>22</sub>) is the estimated coefficient for the factor X<sub>i</sub>. The main effect (X<sub>1</sub> and X<sub>2</sub>) represents the average results of changing one factor at a time from its low to high values. The interaction term (X<sub>1</sub>X<sub>2</sub>) show how the response changes, when 2 factors are changed simultaneously. The polynomial term (X<sub>1</sub><sup>2</sup> and X<sub>2</sub><sup>2</sup>) are included to investigate nonlinearity. The t<sub>50%</sub>, Q<sub>12</sub> and Q<sub>6</sub>, for 9 batches (CFT1-CFT9) showed a wide variation (i.e. 40.2 - 454.3 min, 71.74 - 99.46, 41.0 - 78.7 min respectively). The responses of formulation prepared by 3<sup>2</sup> factorial designs are indicated in Table 2. The data clearly indicate that the t<sub>50%</sub>, Q<sub>12</sub> and Q<sub>6</sub> were strongly dependent on the selected independent variables. The fitted equation relating the response t<sub>50%</sub>, Q<sub>12</sub> and Q<sub>6</sub> to the transformed factors are, t<sub>50%</sub> = 266.63 - 80.4833X<sub>1</sub> + 142.85X<sub>2</sub> (R<sup>2</sup> = 0.9133)

$$Q_{12} = 82.34 + 5.9262X_1 - 9.5363X_2 \text{ (R}^2 = 0.8472\text{)} \text{ and } Q_6 = 58.45 + 7.3500X_1 - 13.1833X_2 \text{ (R}^2 = 0.9337\text{)}.$$

The values of the correlation coefficient indicate a good fit. (**Fig 5, 6, 7.**) shows the plot of the amount of citric acid (X<sub>1</sub>) and amount of HPMC K100M (X<sub>2</sub>) versus t<sub>50%</sub>, Q<sub>12</sub> and Q<sub>6</sub> respectively. The data demonstrate that both X<sub>1</sub> and X<sub>2</sub> affect the drug release (t<sub>50%</sub>, Q<sub>12</sub> and Q<sub>6</sub>). It was concluded that the low level of X<sub>1</sub> (amount of citric acid) and the higher level of X<sub>2</sub> (amount of HPMC K100M) favor the preparation of floating sustained release cephalixin tablets. The high value of X<sub>1</sub>X<sub>2</sub> coefficient also suggests that the interaction between X<sub>1</sub> and X<sub>2</sub> has a significant effect on t<sub>50%</sub>. An increase in the concentration of citric acid (X<sub>1</sub>) and amount of HPMC K100M (X<sub>2</sub>), decrease rate of release of cephalixin floating tablet respectively. All the tablets of factorial design batches showed good in vitro buoyancy, having floating lag time between 40 - 60 sec and remaining buoyant for 12 hours. The bulk density of granules was found to be between 0.3061 ± 0.04 to 0.3658 ± 0.07 g/cm<sup>3</sup>. This indicates good packing capacity of granules. Carr's index was found to be between 14.89 ± 0.03 to 20 ± 0.10 showing good flow characteristics. Hausner ratio low range was indicates good flowability. The angle of repose of all the formulations within the range of 16.09 ± 0.08 to 21.96 ± 0.12 i.e. granules were of good flow properties.

All the formulations from batch CFT1 to CFT9 were evaluated with Thickness and diameter of tablets, measured by vernier caliper. Thickness and diameter was in range of 4.85 ± 0.04 to 5.30 ± 0.05. The hardness of tablet was in range of 13 ± 0.23 to 13 ± 0.40 measured by Monsanto hardness tester. The friability was in range of 0.0010 ± 0.02 to 0.0027 ± 0.01. The values of average weight are within limit. Drug content was in range of 99.63 ± 0.12 to 115.73 ± 0.13 indicating good content uniformity in the prepared formulation results shown in (**Table 3**).

In Vitro Buoyancy Studies conducted, the gas generated is trapped and protected within the gel, formed by hydration of polymer, thus decreasing the density of the tablet. As the density of the tablet falls below 1, the tablet became buoyant. In Vitro Buoyancy Studies Floating lag time was in range of 40sec to 60sec results shown in Photographs (**Fig. 8**).

The swelling index was calculated with respect to time. As time increase, the swelling index was increased, because weight gain by tablet was increased proportionally with rate of hydration. Later on, it decreased gradually due to dissolution of outermost gelled layer of tablet into dissolution medium. The direct relationship was observed between swelling index and HPMC K100M concentration and as HPMC K100M concentration increase, swelling index was increased shown in **(Fig. 9)**.

From the dissolution study of batch CFT1 to CFT9, it was concluded that release from the matrix is largely dependent on the polymer swelling, drug diffusion and matrix erosion. The drug release study was carried out up to 12 hrs. The percentage drug release from batch CFT1 to CFT9 vary from 72.28 to 99.461 %. Large concentration of high viscosity polymer induces the formation of strong viscous gel layer that slowed down the rate of water diffusion into the tablet matrix, which may result in the retardation or decreases the drug release (CFT3). Dissolution profile for all batches were shown in **(Fig. 10)**. All these formulations presented a dissolution behavior controlled by anomalous transport mechanism, when treated with kinetic equations and cephalixin

release from hydrophilic binder matrices followed Fickian diffusion shown in **(Table 4)**. The SEM images of the tablet showed a network in the swollen polymer through which the drug diffused to the surrounding medium and intact surface without any perforations, channels, or troughs shown in **(Fig. 11)**

### CONCLUSION

A systemically study using a  $3^2$  full factorial design revealed that the amount of citric acid ( $X_1$ ) and amount of hydroxyl propyl methyl cellulose (HPMC K100M) ( $X_2$ ) had a significantly effect on  $t_{50\%}$ ,  $Q_{12}$  and  $Q_6$ . The formulation CFT6 was selected as an optimized formulation because it gave the best results in terms of the required in vitro buoyancy study, good matrix integrity and drug release in sustained release manner. In dissolution study of all formulation it was observed that by increasing concentration of polymer, release rate of drug was retarded. All the formulations were presented a dissolution behavior controlled by anomalous transport mechanism, It also followed best-fit model for all batches were the peppas and matrix kinetic model. Thus, it was concluded that the drug was released from matrix by diffusion mechanism.

**Table 1: Composition of Floating Tablets of Cephalixin**

Ingredient (mg)	CFT1	CFT2	CFT3	CFT4	CFT5	CFT6	CFT7	CFT8	CFT9
Cephalixin	500	500	500	500	500	500	500	500	500
HPMC K100M	100	125	150	100	125	150	100	125	150
Sodium bicarbonate	150	150	150	150	150	150	150	150	150
Citric acid	15	15	15	20	20	20	25	25	25
Microcrystalline cellulose	50	50	50	50	50	50	50	50	50
PVK-K30	40	40	40	40	40	40	40	40	40
Magnesium stearate	15	15	15	15	15	15	15	15	15
Talc	10	10	10	10	10	10	10	10	10
Total weight of tablets	880	905	930	885	910	935	890	915	940
<b>Floating lag time in sec.</b>	<b>45</b>	<b>45</b>	<b>60</b>	<b>50</b>	<b>45</b>	<b>40</b>	<b>60</b>	<b>50</b>	<b>55</b>

**Table 2: Formulation and Dissolution Characteristics of Batches in 3<sup>2</sup> Factorial Designs**

Batch code	Coded values		t <sub>50%</sub> (min)	% release at 6hr (Q <sub>6</sub> )	% release at 12hr(Q <sub>12</sub> )
	X1	X2			
CFT1	-1	-1	234.8	61.9	87.87
CFT2	-1	0	383.9	48.4	71.74
CFT3	-1	+1	454.3	41.01	72.28
CFT4	0	-1	40.2	78.7	94.59
CFT5	0	0	254.1	57.2	73.92
CFT6	0	+1	442.3	43.5	73.24
CFT7	+1	-1	61.0	78.1	99.46
CFT8	+1	0	232.6	62.2	88.89
CFT9	+1	+1	296.5	55.1	79.14

**Translation of Coded Values to Actual Values**

Coded values	Actual values	
	X <sub>1</sub>	X <sub>2</sub>
-1	15	100
0	20	125
+1	25	150

\*Where X<sub>1</sub> - Amount of citric acid, X<sub>2</sub> - Amount of HPMC K100 M., t<sub>50%</sub> - time required for 50% of drug release, Q<sub>12</sub> - percentage drug release at 12 hours, Q<sub>6</sub> - percentage drug release at 6 hours.

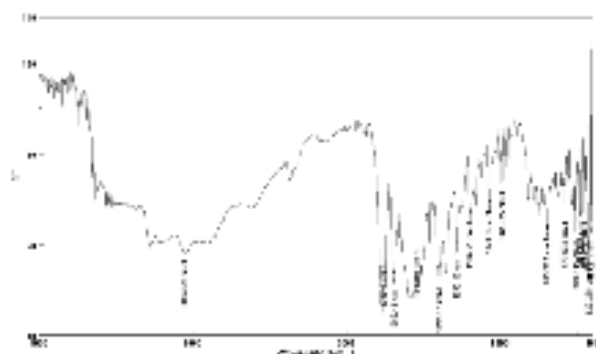
**Table 3: Tablet Properties of Cephalexin Floating Tablets**

Batch code	Average wt(mg)	Thickness (mm)	Diameter (mm)	Hardness (kg/cm <sup>2</sup> )	Friability (%)	Drug content (%)
CFT1	878.65	4.85 ± 0.04	13.11 ± 0.05	13 ± 0.32	0.0027 ± 0.01	102.08 ± 0.13
CFT2	906.00	4.88 ± 0.02	13.07 ± 0.02	13 ± 0.40	0.0019 ± 0.06	99.63 ± 0.12
CFT3	932.25	5.05 ± 0.07	13.06 ± 0.04	13 ± 0.23	0.0019 ± 0.04	104.71 ± 0.22
CFT4	887.50	4.78 ± 0.02	13.07 ± 0.07	13 ± 0.40	0.0024 ± 0.02	106.91 ± 0.15
CFT5	914.10	4.90 ± 0.04	13.06 ± 0.02	13 ± 0.27	0.0021 ± 0.07	107.47 ± 0.10
CFT6	939.65	5.07 ± 0.02	13.05 ± 0.09	13 ± 0.35	0.0010 ± 0.02	108.44 ± 0.12
CFT7	882.40	4.85 ± 0.07	13.10 ± 0.03	13 ± 0.28	0.0018 ± 0.05	103.36 ± 0.14
CFT8	917.65	4.98 ± 0.04	13.07 ± 0.05	13 ± 0.39	0.0015 ± 0.08	115.73 ± 0.13
CFT9	942.15	5.30 ± 0.05	13.01 ± 0.07	13 ± 0.25	0.0014 ± 0.06	106.28 ± 0.10

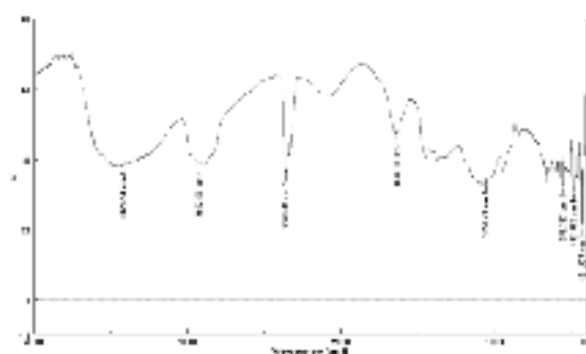
\*All readings are average ± (SD)

**Table 4: Release kinetics for Korsmeyer- Peppas Model**

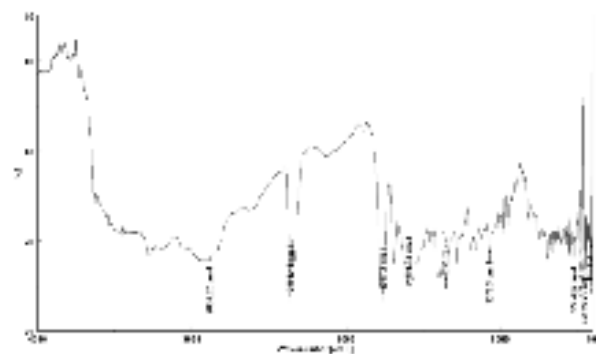
Formulations	n	k	r	Best fit model
CFT1	0.3318	9.0500	0.9401	Matrix
CFT2	0.5274	2.2115	0.9926	Matrix
CFT3	0.8511	0.2737	0.9973	Peppas
CFT4	0.2067	23.307	0.9587	Peppas
CFT5	0.3874	5.8499	0.9926	Peppas
CFT6	0.6752	0.8175	0.9975	Peppas
CFT7	0.2511	17.808	0.9630	Peppas
CFT8	0.4053	5.8056	0.9856	Matrix
CFT9	0.3885	5.7085	0.9835	Matrix



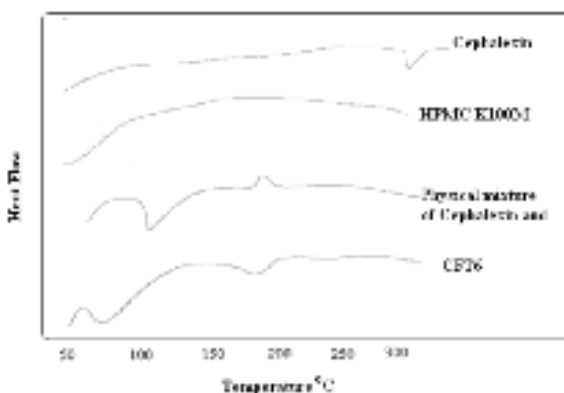
**Fig. 1: FTIR spectral analysis of Cephalexin**



**Fig. 2: FTIR spectral analysis of HPMC K100M**



**Fig. 3: FTIR spectral analysis of Physical Mixture**



**Fig. 4: DSC thermogram of HPMC K100M; Cephalexin; Physical mixture; CFT6 Optimized formulation**

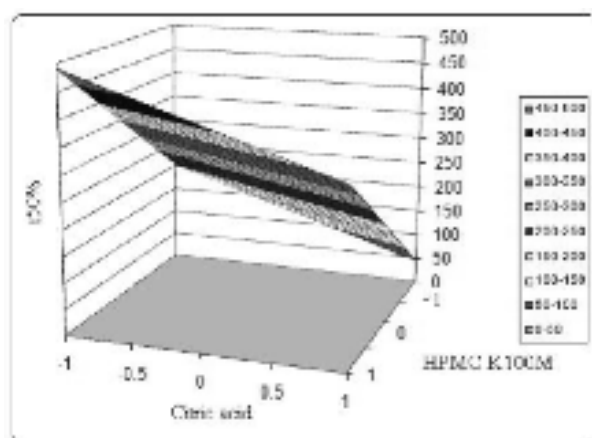


Fig. 5: Response surface plot for  $t_{90\%}$

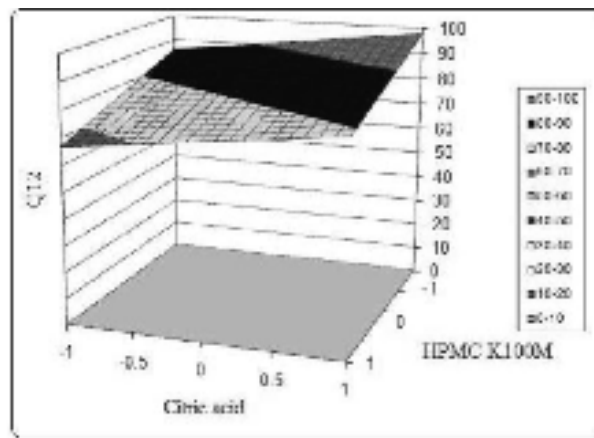


Fig. 6: Response surface plot for  $Q_1$

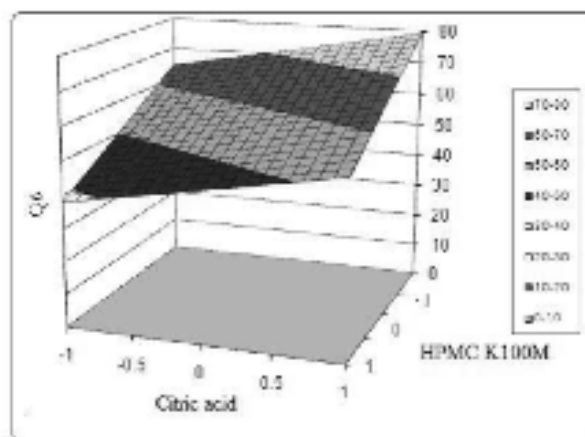


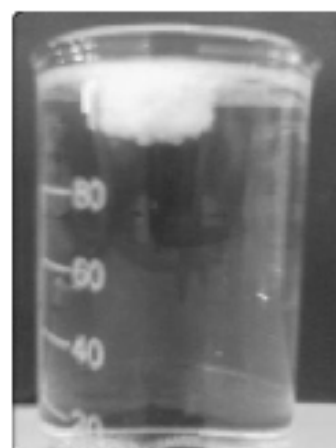
Fig. 7: Response surface plot for  $Q_2$



CFT6 after 0 min



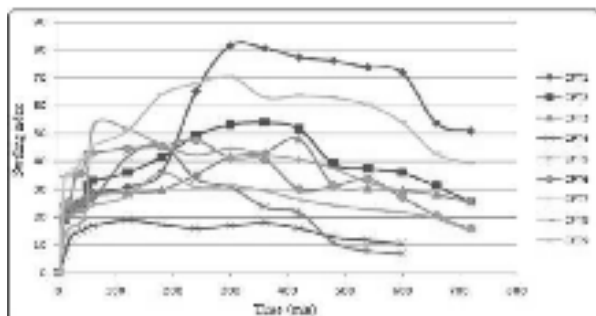
CFT6 after 40 sec



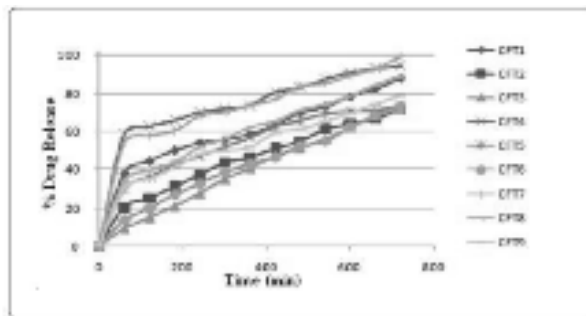
CFT6 after 1 min

Fig. 8: Photograph of in vitro buoyancy study of CFT6 batch

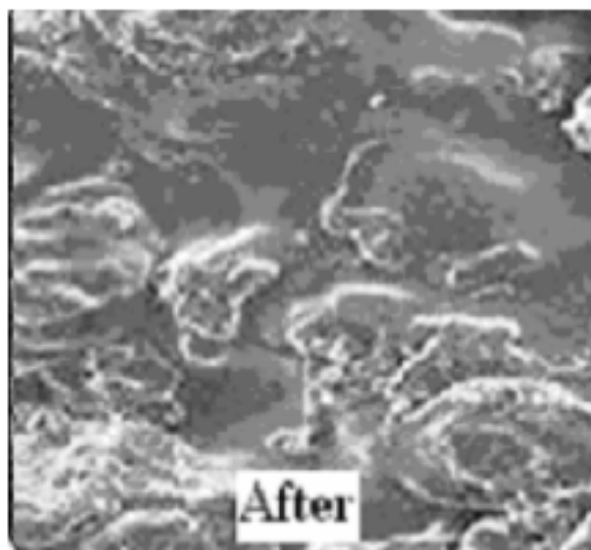
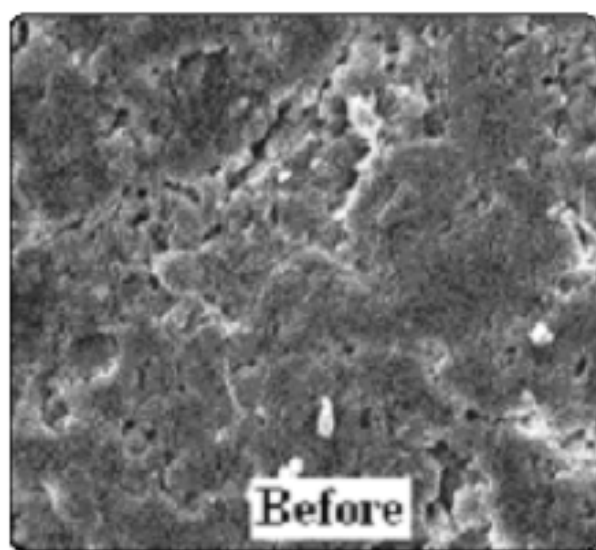




**Fig. 9: Relationship between swelling index and time**



**Fig. 10: Results of % drug release Vs time**



**Fig.11: Scanning electron microscopy images of tablet surfaces before and after Dissolution Original magnification X 1,000**

## REFERENCES

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